## Estimating the interfacial permeability for flow into a poroelastic medium

Zelai Xu<sup>1</sup>, Pengtao Yue<sup>2</sup>, and James J. Feng<sup>1,3</sup>

<sup>1</sup>Department of Chemical and Biological Engineering, University of British Columbia, Vancouver, BC V6T 1Z3, Canada <sup>2</sup>Department of Mathematics, Virginia Tech, Blacksburg, VA 24061, USA <sup>3</sup>Department of Mathematics, University of British Columbia, Vancouver, BC V6T 1Z2, Canada

## Abstract

Boundary conditions between a porous solid and a fluid has been a long-standing problem in modeling porous media. For deformable poroelastic materials such as hydrogels, the question is further complicated by the elastic stress from the solid network. Recently, an interfacial permeability condition has been developed from the principle of positive energy dissipation on the hydrogel-fluid interface. Although this boundary condition has been used in flow computations and yielded reasonable predictions, it contains an interfacial permeability  $\eta$  as a phenomenological parameter. In this work, we use pore-scale models of flow into a periodic array of solid cylinders or parallel holes to determine  $\eta$  as a function of the pore size and porosity. This provides a means to evaluate the interfacial permeability for a wide range of poroelastic materials, including hydrogels, foams and biological tissues, to enable realistic flow simulations.

Introduction. Flow through a deformable porous medium can be described by a poroelasticity model. This is essentially a mixture model that views the solid and the fluid as interpenetrating continua, each phase being described by its own volume fraction, velocity and stress that obey continuity and momentum equations for each phase [1-3]. Since the model erases all pore-scale geometric information about the fluid-solid boundaries, and instead poses momentum equations for both phases over the entire porous medium, additional boundary conditions (BCs) must be supplied to make the problem solvable [4,5]. This issue arises in soft porous media such as hydrogels, foams, flocculated fiber suspensions and biological tissues. For brevity, we will refer to our media only as "hydrogels" or "gels" hereafter. Even for rigid porous media, where the solid stress becomes indeterminate, a similar question arises, albeit in a different form [6,7].

The mathematical structure of the problem can be appreciated from a simplified onedimensional (1D) flow (Fig. 1). The general vectorial forms of the governing equations and BCs can be found in Xu *et al.* [8]. A uniform flow of a solvent of viscosity  $\mu$ encounters a layer of hydrogel whose downstream surface is fixed in space. On the upstream interface, the fluid experiences a contraction flow into the pores. Inside the gel layer, the fluid exerts a Darcy drag on the solid, and compresses the gel layer into a steady state. The poroelastic model for this steady state can be reduced to the following



Figure 1: A one-dimensional (1D) flow into a hydrogel for illustrating the interfacial permeability boundary condition of Eq. (6).

1D form [8]:

$$(\phi_f v_f)' = 0, \tag{1}$$

$$p' = -\frac{\mu}{k}\phi_f v_f + \frac{1}{\phi_f}(\phi_f \sigma_f)', \qquad (2)$$

$$p' = (\phi_f \sigma_f + \phi_s \sigma_s)', \tag{3}$$

where the prime indicates the spatial derivative d/dx,  $\phi_f$  and  $\phi_s = 1 - \phi_f$  are the fluid and solid volume fractions, p is the pressure inside the gel, shared by the fluid and the solid phases,  $v_f$  is the fluid pore velocity, and  $\sigma_f$  and  $\sigma_s$  are respectively the fluid and solid normal stresses in the x direction. Equation (1) is the fluid continuity equation. Equation (2) is the Brinkman extension of Darcy's law for the fluid flow. The permeability k is a function of the local porosity, a commonly used form being the Kozney-Carman model [3,9]. Finally, Eq. (3) is the total momentum balance on the two phases. For the viscous solvent,  $\sigma_f = 2\mu v'_f$ . For the solid,  $\sigma_s$  is given by a linearly elastic or hyperelastic constitutive equation [8].

On the upstream interface, volume conservation and traction balance give us two BCs:

$$\phi_f v_f = V_0, \tag{4}$$

$$-\phi_f \sigma_f - \phi_s \sigma_s = P, \tag{5}$$

where  $V_0$  and P are the uniform velocity and pressure upstream of the interface. For a hydrogel, an additional BC is required, and Young *et al.* [8, 10, 11] have derived the following based on the principle of positive energy dissipation on the fluid-gel interface:

p

$$V_0 - v_f = \eta \left( P - p + \sigma_s \right),\tag{6}$$

with  $\eta > 0$  being the interfacial permeability. At the downstream interface, we impose zero solid displacement ( $u_s = 0$ ) and zero fluid stress. The permeability BC of Eq. (6) is intuitive with the normal velocity jump proportional to the normal stress jump across the interface. It has also produced reasonable results in flow computations through hydrogels [5, 8, 12]. Nevertheless,  $\eta$  remains a phenomenological coefficient that has never been measured experimentally. For realistic flow simulations, it will be desirable to know its value for specific poroelastic media.

Pore-scale models. To estimate  $\eta$ , we adopt an idea from pore-scale models for rigid porous media. Many authors have calculated the bulk permeability of rigid porous media by the tube-bundle model [9,13,14] or by flow around periodic arrays of solid cylinders or spheres [9,15–18]. The solid-array representation has also been used to explore the interfacial conditions [6,7,16,17,19–21]. We can use such a *rigid* pore model to estimate  $\eta$  for our poroelastic medium insofar as we seek a constitutive relation for  $\eta$  as a function of the steady-state local porosity  $\phi_f$  and pore size r. The compression that has produced such a steady state and the fact that  $\phi_f$  and r may vary in the bulk of the medium are of no immediate import to our purpose.

Another issue is that the BC of Eq. (6) involves the solid stress  $\sigma_s$ , which is undefined for rigid solids. We bypass this obstacle by eliminating  $\sigma_s$  using the total traction balance of Eq. (5). Furthermore, we eliminate  $v_f$  in favor of  $V_0$  by the volume conservation of Eq. (4) to arrive at the following interfacial permeability BC:

$$V_0 = \eta \frac{\phi_f^2}{\phi_s^2} (P - p + \sigma_f) = \frac{\tilde{\eta}}{\mu} (P - p + \sigma_f) \approx \frac{\tilde{\eta}}{\mu} (P - p), \tag{7}$$

where we have simplified the notation by introducing the *penetration length*  $\tilde{\eta} = \eta \mu \phi_f^2 / \phi_s^2$ . This removes the viscosity dependence and leaves  $\tilde{\eta}$  a geometric parameter, akin to the Navier slip length or the "transpiration length" [7]. We have further dropped the viscous normal stress  $\sigma_f$  as it is typically much smaller than the friction that gives rise to the Darcy drag and the entry pressure drop P - p [22,23]. Now we can use a pore model to compute the entry pressure drop and back out the interfacial penetration length  $\tilde{\eta}$  and the interfacial permeability  $\eta$ .

It is interesting to note the similarity between the permeability BC of Eq. (7) and the pressure jump BCs for rigid porous media [6, 7, 20]. For example, Lācis *et al.* [7] proposed the following form (in our notation):

$$V_0 = -\frac{1}{f}(P - p + \sigma_f),\tag{8}$$

where the "resistance coefficient" f represents the friction force against the solvent passing through the interface. Although Eqs. (7) and (8) have come from different physical arguments, they are algebraically similar, and both recognize the need for an interfacial pressure drop to overcome the resistance to the fluid entering the pores. This idea deviates from the long-standing assumption of traction continuity or pressure continuity at the interface [21, 22, 24–26]. Lācis *et al.* [7] further used numerical computation in a periodic pore model to evaluate f, and we will be able to compare our result quantitatively with theirs.

We use four geometric representations for the porous material (Fig. 2a): semi-infinite arrays of circular and square cylinders aligned in the flow direction, and parallel circular and square holes in a semi-infinite solid. In either case, the cylinders or holes are arranged in a periodic square lattice on the cross-section of the medium. Thus, the solvent coming from the left of Fig. 1 experiences a contraction flow to enter the "pores".

These geometries are inspired by prior models for porous medium, e.g., [15–19], but with one important difference. Prior models specify a periodicity along the *depth* of the porous medium (i.e., the x-axis of Fig. 1). Then ambiguities arise as to where to place the interface, and how many periods to use for spatial averaging. Depending on whether the nominal interface cuts through the solid objects [15,16], stays tangential to their apex in the top foremost row [19,27], or is placed further in the bulk fluid [7,17], the continuumlevel result may differ greatly. Furthermore, James and Davis [19] demonstrated that a shear flow penetrates only the first row of cylinders. This challenges the scale-separation assumption underlying the continuum Brinkman or Darcy model [7]. Our setups avoid both difficulties; the semi-infinite cylinders or holes present a clear-cut interface, and they have "pre-averaged" the spatial variations in the depth direction. Experimentally, Tachie *et al.* [28, 29] tested brush models that resemble our setup, although they only considered shear flows past the top of the transverse posts. Our results will turn out to



Figure 2: (a) The interface for four pore geometries, with periodic arrays of circular and square cylinders and circular and square holes. The grey and white areas represent the solid and pore space, the latter occupying an area fraction that equals  $\phi_f$ . The dashed squares, of edge length r, represent the cross-sections of our computational domain. (b) The computational domain for Stokes flow entering a pore between square cylinders, with its cross-section at the interface corresponding to the dashed square above. The flow is depicted by velocity vectors.

be largely insensitive to the geometric details of the model (Fig. 3 below), and thus we will not consider other solid shapes or other spatial arrangements [15, 19].

Numerical and theoretical results. Taking advantage of spatial periodicity and symmetry, we solve the 3D Stokes flow in a computational domain that corresponds to a quarter of a single pore; Fig. 2(b) shows an example for the square cylinder. The 3D pore-scale flow will be processed to yield the interfacial penetration of the 1D setup on the continuum level (Fig. 1). We impose no-slip conditions on the solid surfaces and symmetry conditions on all fluid boundaries. The upstream boundary has a uniform incoming flow at velocity  $V_0$  and the downstream boundary has stress-free conditions. The finite-element code is based on the open-source finite-element library deal.II. Mesh refinement has confirmed adequate numerical resolution. The up- and downstream boundaries are each 4r away from the opening of the pore so they have negligible effect on the contraction flow and the final result.

To compute the interfacial pressure drop P - p of Eq. (7), we identify P with the upstream pressure  $P_0$  in our pore model, and p with the averaged pore pressure at the opening of the pore:  $p_f = \int_{A_c} p \, dA/(r^2 \phi_f)$ , where  $A_c$  is the cross-section of the interface excluding the solid portion (the shaded area of Fig. 2b). Dimensional analysis dictates

$$V_0 = \frac{r(P_0 - p_f)}{\mu} \psi(\phi_f),$$
(9)

where  $\psi(\phi_f)$  is a dimensionless function that we have determined numerically and plotted in Fig. 3. As expected,  $\psi$  decreases toward zero as  $\phi_f \to 0$  and increases with  $\phi_f$ .



Figure 3: The function  $\psi(\phi_f)$  obtained by computing the Stokes flow into the model porous medium of figure 2 with different geometries. The solid curve represents the  $\psi_1(\phi_f)$  function of Eq. (12), while the dashed curve  $\psi_2(\phi_f)$  of Eq. (13).

Furthermore,  $\psi$  differs little among the four geometries tested, suggesting that they are all robust and realistic representations of the interfacial property of a porous medium. On the continuum level, therefore,  $\phi_f$  is the main geometric parameter that matters. The numerical data in Fig. 3 embody the idea that an interfacial pressure drop is needed to propel the fluid into the pores; it is essentially the excess pressure in entry flow [30].

To complement the numerical results, we can estimate theoretically the viscous dissipation of the entry flow, under the following two assumptions:

- The dissipation mostly occurs in an entry region  $\Omega$  extending a distance of r upstream from the interface, based on the perturbed flow field of Fig. 2(b).
- The dissipation is mostly attributable to  $v_x$ , the x-component of the velocity.

The longitudinal velocity accelerates from  $V_0$  at the upstream surface of  $\Omega$  to  $V_0/\phi_f$ at the interface, suggesting a strain rate  $\partial v_x/\partial x \sim (V_0/\phi_f - V_0)/r = V_0\phi_s/(r\phi_f)$ . To account for the 3D nature of the flow, we introduce a fitting parameter C such that  $\partial v_x/\partial x = CV_0\phi_s/(r\phi_f)$ . Similarly, we estimate the shear rates using the averaged velocity  $V_0/\phi_f$  divided by the pore size r:  $\partial v_x/\partial y = \partial v_x/\partial z = CV_0/(\phi_f r)$ . Therefore, the total viscous dissipation inside  $\Omega$  is

$$I_{v} = \mu \Omega \left\{ 2 \left( \frac{\partial v_{x}}{\partial x} \right)^{2} + \left[ \left( \frac{\partial v_{x}}{\partial y} \right)^{2} + \left( \frac{\partial v_{x}}{\partial z} \right)^{2} \right] \right\} = 2C^{2} \mu V_{0}^{2} r \left( \frac{\phi_{s}^{2} + 1}{\phi_{f}^{2}} \right).$$
(10)

Meanwhile, the pressure work on the entrance of  $\Omega$  is  $PV_0r^2$ , and that on the exit of  $\Omega$  is  $-p_f(V_0/\phi_f)(r^2\phi_f)$ . Equating the total work  $(P - p_f)V_0r^2$  to the viscous dissipation, we have

$$V_0 = \frac{r(P - p_f)}{2C^2\mu} \frac{\phi_f^2}{\phi_s^2 + 1},\tag{11}$$

and in turn the following approximation to the  $\psi(\phi_f)$  function of Eq. (9):

$$\psi_1(\phi_f) = \frac{1}{2C^2} \frac{\phi_f^2}{\phi_s^2 + 1}.$$
(12)

 $C = 1/\sqrt{2} \approx 0.707$  gives a good fit to the numerical data of Fig. 3. Considering the simplicity of the estimation, the semi-analytical  $\psi_1(\phi_f)$  captures the numerical data

well. The greatest discrepancy appears at the dilute limit  $\phi_f \to 1$ ; some numerical data turn upward whereas the formula remains concave. This discrepancy can be understood as an effect of the pore geometry in the limit of  $\phi_f \to 1$ , in an exception to our earlier statement on the insensitivity to pore geometry. For flow along a cylinder, the crosssectionally averaged shear stress vanishes as the cylinder becomes thinner. This explains the upturn in the numerical data for cylinders in Fig. 3. Conversely, for flow in a hole, the average shear stress stays finite when the wall become thinner. This difference is noticeable among the numerical data of Fig. 3. Our estimation of the shear rates  $\partial v_x / \partial y = \partial v_x / \partial z = CV_0/(\phi_f r)$  remains finite as  $\phi_f \to 1$ . Thus, it reflects internal flow in holes, not external flow along cylinders.

As an alternative, we can estimate the average shear rate in the external axial flow along an infinite circular cylinder, with its analytical logarithmic velocity profile. Recalculating the viscous dissipation in  $\Omega$ , we arrive at the following formula:

$$\psi_2(\phi_f) = \frac{1}{2C^2} \frac{\phi_f^2}{\phi_s^2 + \phi_f^2 q^2/2}, \text{ with } q(\phi_s) = \frac{8\sqrt{\pi} (\sqrt{\phi_s} - 1)^2 (\sqrt{\phi_s} + 2)}{3(2\ln\phi_s - 4\phi_s + \phi_s^2 + 3)}.$$
 (13)

This  $\psi_2(\phi_f)$  function is plotted as the dashed line in Fig. 3 by taking the same fitting parameter  $C = 1/\sqrt{2}$ . It accurately captures the numerical results for the cylinder setup, including the sharp increase near the limit  $\phi_f \to 1$ . But for lower porosities, it underpredicts the data for the hole setup. Either  $\psi_1(\phi_f)$  or  $\psi_2(\phi_f)$  serves as an adequate representation of the interfacial permeability. They are counterparts of the two formulas for the bulk permeability k, the Kozeny-Carman formula based on flow in conduits, and the Brinkman formula on external flow around solid objects [9]. As a further test, we have numerically computed the viscous dissipation incurred by the contraction flow, and the  $\psi$  function thus obtained agrees with the numerical data of Fig. 3 to within the difference among the pore geometries.

From  $\psi$  we can estimate the interfacial penetration length of Eq. (7),

$$\tilde{\eta} = \psi(\phi_f)r,\tag{14}$$

and in turn the interfacial permeability  $\eta$ . Thus,  $\psi = \tilde{\eta}/r$  is the dimensionless interfacial penetration length scaled by the pore size. A slightly different scaling,  $\tilde{\eta}/\sqrt{k}$ , can be interpreted as the ratio between the interfacial permeability and the bulk permeability. We can now use Eq. (14) and Fig. 3 to estimate  $\tilde{\eta}$  for real materials. Most hydrogels have small pores (nm to micron scale) [31–33] and high porosity  $\phi_f > 0.9$  [33–36]. Thus,  $\tilde{\eta}$  can range from r up to 4r. For low-swelling-ratio gels [37], biological tissues [38], larger-scale porous media such as foam [39] and packed beds of soft particles [40],  $\phi_f$ can be as low as 0.5, and  $\tilde{\eta}$  will be on the order of 0.1r.

Lācis *et al.* [7] computed the f factor in Eq. (8) numerically in a lid-driven flow over a model porous medium. A direct comparison can thus be made with our  $\psi$  of Fig. 3. For  $\phi_f = 0.75$ , they reported  $f = -5.215\mu/r$  for a square array of circular cylinders aligned in the vortex direction of the flow outside. This translates to a penetration length  $\tilde{\eta}/r = 0.192$ , smaller than our  $\psi(\phi_f = 0.75) = 0.367$ , but on the same order of magnitude. The quantitative discrepancy may have been due to differences in the geometric and flow setup. For example, theirs was a planar 2D flow around the crosssections of cylinders, while ours is a 3D axial flow. Their interface was placed in the bulk of the clear fluid, 0.2r outside the plane tangential to the first row of cylinders, whereas our interface is flush with the ends of the semi-infinite cylinders and holes. Their pressure difference was volume-averaged, going 4 periodic cells into the depth of the porous medium, while our  $p_f$  is surface-averaged on the interface. Finally, their liddriven flow is 2D on the continuum level, with variations along the interface, whereas our setup mimics the simpler 1D compression of Fig. 1. Such differences notwithstanding, both studies support the argument for an interfacial pressure drop. The numerical and semi-analytical results of Fig. 3 can be used to determine the interfacial penetration  $\tilde{\eta}$  and interfacial permeability  $\eta$  for a wide range of porous materials, deformable and rigid alike.

Acknowledgements: J.J.F. acknowledges financial support by Natural Sciences and Engineering Research Council of Canada (Discovery Grants No. 2019-04162, No. 2024-03982, Alliance International Grant No. 586462-23). P.Y. acknowledges the financial support by National Science Foundation (Grants DMS-2012480, DMS-2309732). We thank Neil Balmforth, Uğis Lācis, Arun Ramchandran and Boris Stoeber for helpful discussions.

## References

- R. Burridge, J. B. Keller, Poroelasticity equations derived from microstructures, J. Acoust. Soc. Am. 70 (1981) 1140–1146.
- [2] J. M. Carcione, Chapter 7 Biot theory for porous media, in: Wave Fields in Real Media, 3rd Edition, Elsevier, Oxford, 2015, pp. 299 – 420.
- [3] C. W. MacMinn, E. R. Dufresne, J. S. Wettlaufer, Large deformations of a soft porous material, Phys. Rev. Appl. 5 (2016) 044020.
- [4] M. Minale, Momentum transfer within a porous medium. II. Stress boundary condition, Phys. Fluids 26 (2014) 123102.
- [5] L. Li, J. Zhang, Z. Xu, Y.-N. Young, J. J. Feng, P. Yue, An arbitrary Lagrangian-Eulerian method for simulating interfacial dynamics between a hydrogel and a fluid, J. Comput. Phys. 451 (2022) 110851.
- [6] T. Carraro, C. Goll, A. Marciniak-Czochra, A. Mikelić, Pressure jump interface law for the Stokes-Darcy coupling: confirmation by direct numerical simulations, J. Fluid Mech. 732 (2013) 510–536.
- [7] U. Lācis, Y. Sudhakar, S. Pasche, S. Bagheri, Transfer of mass and momentum at rough and porous surfaces, J. Fluid Mech. 884 (2020) A21.
- [8] Z. Xu, J. Zhang, Y.-N. Young, P. Yue, J. J. Feng, A comparison of four boundary conditions for the fluid-hydrogel interface, Phys. Rev. Fluids 7 (2022) 093301.
- [9] F. A. L. Dullien, Chapter 3: Single-phase transport phenomena in porous media, in: Porous Media: Fluid Transport and Pore Structure, 2nd Edition, Academic Press, San Diego, 1992, pp. 237–317.
- [10] Y.-N. Young, Y. Mori, M. J. Miksis, Slightly deformable Darcy drop in linear flows, Phys. Rev. Fluids 4 (2019) 063601.
- [11] J. J. Feng, Y.-N. Young, Boundary conditions at a gel-fluid interface, Phys. Rev. Fluids 5 (2020) 124304.
- [12] Z. Xu, P. Yue, J. J. Feng, Poroelastic modeling reveals the cooperation between two mechanisms for albuminuria, J. R. Soc. Interface 20 (2023) 20220634.
- [13] J. T. Bartley, D. W. Ruth, Relative permeability analysis of tube bundle models, Transp. Porous Med. 36 (1999) 161–188.

- [14] H. K. Dahle, M. A. Celia, S. M. Hassanizadeh, Bundle-of-tubes model for calculating dynamic effects in the capillary-pressure-saturation relationship, Transp. Porous Med. 58 (2005) 5–22.
- [15] R. E. Larson, J. J. L. Higdon, Microscopic flow near the surface of two-dimensional porous media. Part 1. Axial flow, J. Fluid Mech. 166 (1986) 449–472.
- [16] R. E. Larson, J. J. L. Higdon, Microscopic flow near the surface of two-dimensional porous media. Part 2. Transverse flow, J. Fluid Mech. 178 (1987) 119–136.
- [17] A. S. Sangani, S. Behl, The planar singular solutions of Stokes and Laplace equations and their application to transport processes near porous surfaces, Phys. Fluids A 1 (1989) 21–37.
- [18] N. Martys, D. P. Bentz, E. J. Garboczi, Computer simulation study of the effective viscosity in Brinkman's equation, Phys. Fluids 6 (1994) 1434–1439.
- [19] D. F. James, A. M. Davis, Flow at the interface of a model fibrous porous medium, J. Fluid Mech. 426 (2001) 47–72.
- [20] T. Carraro, C. Goll, A. Marciniak-Czochra, A. Mikelić, Effective interface conditions for the forced infiltration of a viscous fluid into a porous medium using homogenization, Comput. Methods Appl. Mech. Eng. 292 (2015) 195–220.
- [21] U. Lācis, S. Bagheri, A framework for computing effective boundary conditions at the interface between fluid and a porous medium, J. Fluid Mech. 812 (2017) 866–889.
- [22] S. Haber, R. Mauri, Boundary conditions for Darcy's flow through porous media, Int. J. Multiphase Flow 9 (1983) 561–574.
- [23] O. Coussy, Poromechanics, Wiley, 2004.
- [24] J. Koplik, H. Levine, A. Zee, Viscosity renormalization in the brinkman equation, Phys. Fluids 26 (1983) 2864–2870.
- [25] J. H. Masliyah, G. Neale, K. Malysa, T. G. M. Van De Ven, Creeping flow over a composite sphere: Solid core with porous shell, Chem. Eng. Sci. 42 (1987) 245–253.
- [26] U. Lācis, G. A. Zampogna, S. Bagheri, A computational continuum model of poroelastic beds, Proc. R. Soc. A (2017) 20160932.
- [27] M. F. Tachie, D. F. James, I. G. Currie, Velocity measurements of a shear flow penetrating a porous medium, J. Fluid Mech. 493 (2003) 319–343.
- [28] M. Agelinchaab, M. F. Tachie, D. W. Ruth, Velocity measurement of flow through a model three-dimensional porous medium, Phys. Fluids 18 (2006) 017105.
- [29] J. K. Arthur, D. W. Ruth, M. F. Tachie, PIV measurements of flow through a model porous medium with varying boundary conditions, J. Fluid Mech. 629 (2009) 343– 374.
- [30] M. A. Rogerson, Y. L. Yeow, Representation of Stokes flow through a planar contraction by Papkovich-Fadle eigenfunctions, Trans. ASME 66 (1999) 940–944.
- [31] M. M. Chui, R. J. Phillips, M. J. McCarthy, Measurement of the porous microstructure of hydrogels by nuclear magnetic resonance, J. Colloid Interface Sci. 174 (1995) 336–344.

- [32] Y.-C. Chiu, M.-H. Cheng, H. Engel, S.-W. Kao, J. C. Larson, S. Gupta, E. M. Brey, The role of pore size on vascularization and tissue remodeling in PEG hydrogels, Biomaterials 32 (2011) 6045–6051.
- [33] A. Salerno, R. Borzacchiello, P. A. Netti, Pore structure and swelling behavior of porous hydrogels prepared via a thermal reverse-casting technique, J. Appl. Polym. Sci. 122 (2011) 3651–3660.
- [34] N. Annabi, J. W. Nichol, X. Zhong, C. Ji, S. Koshy, A. Khademhosseini, F. Dehghani, Controlling the porosity and microarchitecture of hydrogels for tissue engineering, Tissue Eng. B 16 (2010) 371–383.
- [35] Y. Li, O. S. Sariyer, A. Ramachandran, S. Panyukov, M. Rubinstein, E. Kumacheva, Universal behavior of hydrogels confined to narrow capillaries, Sci. Rep. 5 (2015) 17017.
- [36] S. Kovačič, M. S. Silverstein, Superabsorbent, high porosity, PAMPS-based hydrogels through emulsion templating, Macromol. Rapid Commun. 37 (2016) 1814–1819.
- [37] J. Yoon, S. Cai, Z. Suo, R. C. Hayward, Poroelastic swelling kinetics of thin hydrogel layers: comparison of theory and experiment, Soft Matter 6 (23) (2010) 6004.
- [38] R. Penta, L. Miller, A. Grillo, A. Ramírez-Torres, P. Mascheroni, R. Rodríguez-Ramos, Porosity and diffusion in biological tissues. Recent advances and further perspectives, in: J. Merodio, R. Ogden (Eds.), Constitutive Modelling of Solid Continua, Springer International Publishing, Cham, 2020, pp. 311–356.
- [39] T. Lutz, L. Wilen, J. Wettlaufer, A method for measuring fluid pressure and solid deformation profiles in uniaxial porous media flows, Rev. Sci. Instrum. 92 (2021) 025101.
- [40] D. R. Hewitt, J. S. Nijjer, M. G. Worster, J. A. Neufeld, Flow-induced compaction of a deformable porous medium, Phys. Rev. E 93 (2016) 023116.